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1 **A comparison between the Compass fundus perimeter and the Humphrey**
2 **Field Analyzer**

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37 Brusini, MD and Luca M. Rossetti are Consultants for CenterVue, Padua, Italy.

38

39 This article contains additional online-only material. The following should appear online-only:
40 Supplementary Figure 1 and 2.

41

42 Running head: Comparison of Compass and Humphrey Field Analyzer

43

44 **Abstract**

45 **Purpose:** To evaluate relative diagnostic precision and test retest variability of two devices,
46 the Compass (CMP, CenterVue, Italy) fundus perimeter and the Humphrey Field Analyzer
47 (HFA, Zeiss, Dublin), in detecting glaucomatous optic neuropathy (GON).

48 **Design:** Multicentre cross-sectional case-control study.

49 **Subjects:** We sequentially enrolled 499 glaucoma patients and 444 normal subjects to analyse
50 relative precision. A separate group of 44 glaucoma patients and 54 normal subjects was
51 analysed to assess test – retest variability.

52 **Methods:** One eye of the recruited subjects was tested with the index tests: HFA (SITA
53 Standard strategy) and CMP (ZEST strategy) with a 24-2 grid. The reference test for GON was
54 specialist evaluation of fundus photographs or OCT, independent of the visual field. For both
55 devices, linear regression was used to calculate the sensitivity decrease with age in the
56 normal group to compute pointwise Total Deviation (TD) values and Mean Deviation (MD).
57 We derived 5% and 1% pointwise normative limits. MD and the total number of TD values
58 below 5% (TD 5%) or 1% (TD 1%) limits per field were used as classifiers.

59 **Main Outcome Measures:** We used partial Receiver Operating Characteristic (ROC) curves
60 and partial Area Under the Curve (pAUC) to compare the diagnostic precision of the devices.
61 Pointwise Mean Absolute Deviation (MAD) and Bland Altman plots for the mean sensitivity
62 (MS) were computed to assess test- retest variability.

63 **Results:** Retinal sensitivity was generally lower with CMP, with an average mean difference of
64 1.85 ± 0.06 dB (Mean \pm Standard Error, $p < 0.001$) in healthy subjects and 1.46 ± 0.05 dB
65 (Mean \pm Standard Error, $p < 0.001$) in patients with glaucoma. Both devices showed similar
66 discriminative power. The MD metric had marginally better discrimination with CMP (pAUC
67 difference \pm Standard Error, 0.019 ± 0.009 , $p = 0.035$). The 95% limits of agreement for the
68 MS were reduced by 13% in CMP compared to HFA in glaucoma subjects, and by 49% in

69 normal subjects. MAD was very similar, with no significant differences.

70 **Conclusions:** Relative diagnostic precision of the two devices is equivalent. Test-retest

71 variability of mean sensitivity for CMP was better than for HFA.

72 Standard Automated Perimetry (SAP) is used to assess the visual field (VF) and is a key
73 examination for detection, diagnosis and follow up in glaucoma. SAP typically uses stimuli of
74 varying intensities to assess the differential light sensitivity at static locations across the VF.
75 The examination demands strong cooperation¹ from test subjects; they are required to
76 maintain central fixation and respond timely and accurately to the presented stimuli. Fixation
77 instability might be an unavoidable feature of a person's vision, especially with advanced age
78 and macular damage². One proposed solution has been to incorporate live fundus tracking in
79 the macular perimetric exam to compensate for eye movements in unstable fixation³.

80 Recently, a novel instrument, the COMPASS fundus perimeter (CMP, CenterVue, Padua, Italy),
81 has successfully employed a live fundus tracking technology for wide field (30 degrees) VF
82 assessment^{4,5} yielding results comparable with the Humphrey Field Analyzer (HFA) in a
83 preliminary study⁴. The CMP captures images of the fundus during the perimetric
84 examination using a scanning laser ophthalmoscope. This design feature is intended to afford
85 compensation for eye movements when the stimuli are presented at predetermined test
86 locations. Moreover, the instrument provides colour images of the fundus and optic nerve that
87 can be mapped to the final perimetric results potentially providing clinically useful
88 information about structure and function in one assessment.

89 Diagnostic accuracy studies are used to certify new examinations before they are brought into
90 clinical practice. The CMP has not yet been scrutinised in this way and this is the main
91 purpose of our investigation. Studies investigating relative diagnostic accuracy are at risk of
92 bias due to shortcomings in design and conduct. For this reason, we designed our study to
93 follow appropriate guidelines on this specific aim^{6,7}.

94 Our cross-sectional and multicentre study was designed to evaluate and compare two index
95 tests, namely the CMP and the HFA. One objective was to evaluate and compare test – retest
96 variability of the two index tests in healthy subjects and patients with glaucomatous optic

97 neuropathy (GON). We hypothesised that the CMP could obtain a 20% reduction in test-retest
98 variability on the measurement of the Mean Sensitivity (MS) of the VF. Another objective was
99 to build a normative database for the CMP and analyse its relative discriminative ability,
100 compared to HFA, in detecting subjects with GON. We specifically hypothesised that the two
101 index tests will have equivalent relative diagnostic precision as assessed by partial area under
102 the receiver operating characteristic (ROC) curve at >75% specificity, across a spectrum of
103 disease severity. In both analyses, the reference assessment for GON was specialist evaluation
104 based on the inspection of fundus photograph or Spectral Domain – Optical Coherence
105 Tomography (SD-OCT) evaluation of the Retinal Nerve Fibre Layer (RNFL), independent of
106 the VF. A further objective was to evaluate examination times for the CMP and HFA.

107

108 **Methods**

109 *Data collection for the normative database and discrimination analysis*

110 People were recruited at eight study sites. These were: ASST - Santi Paolo e Carlo, Milan, Italy;
111 Azienda Ospedaliero Universitaria Santa Maria della Misericordia di Udine, Udine, Italy; NIHR
112 Clinical Research Facility at Moorfields Eye Hospital, London, UK; Department of
113 Ophthalmology and Visual Sciences University of Iowa, 200 Hawkins Drive, Iowa City, IA;
114 Department of Optometry & Vision Sciences, The University of Melbourne,
115 Parkville, Australia; IRCCS Fondazione "G.B. Bietti", Clinica Oculistica Università degli Studi di
116 Roma "La Sapienza", Rome, Italy; and Azienda Ospedaliera Sant'Andrea, Rome, Italy).
117 Recruitment started on 14/09/2015 and concluded on 31/07/2017. Data collection was
118 planned before the index test and reference standard were performed. The study was
119 designed to achieve a target number of 1000 glaucoma subjects and 600 healthy subjects for
120 the normative database and discrimination analysis. However, these targets were not reached
121 by the termination date of the study.

122 Participants eligible for inclusion were consecutive adults (18-90 years) with:

- 123 • Best corrected visual acuity > 0.8 (if ≤ 50 years old) or >0.6 (if >50 years old) in the
124 study eye;
- 125 • Refraction -10D / +6D; astigmatism ±2D;
- 126 • Absence of systemic pathologies that could affect the VF;
- 127 • No use of drugs interfering with the correct execution of the perimetric test;

128 Additional specific inclusion criteria for healthy subjects were:

- 129 • Normal optic nerve head in both eyes (no evidence of excavation, rim narrowing or
130 notching, disc haemorrhages, RNFL thinning);
- 131 • Intraocular Pressure (IOP) less than 21 mmHg in both eyes;

- 132 • No ocular pathologies, trauma, surgeries (apart from uncomplicated cataract surgery)
133 in both eyes;

134 Additional specific inclusion criteria for glaucoma subjects were:

- 135 • GON defined as glaucomatous changes to the optic nerve head (ONH) or retinal nerve
136 fibre layer (RNFL) as determined by a specialist from fundus photograph or SD-OCT,
137 independently of the VF.
- 138 • Patients had to be receiving anti-glaucoma therapy;
- 139 • No ocular pathologies, trauma, surgeries (apart from uncomplicated cataract surgery),
140 other than glaucoma, in both eyes;

141 Eligible patients were identified based on a clinical diagnosis of GON from the clinical registry
142 of the glaucoma clinics in the recruiting centres. An expert clinician confirmed the diagnosis of
143 GON using the imaging data (RNFL SD-OCT or optic nerve photograph) acquired during the
144 protocol examination (see below). Subjects were recruited consecutively. Since the VF metrics
145 were not included in the identification of patients with GON, no stratification was planned
146 according to disease severity.

147 Eligible healthy participants were identified among staff in the clinics, volunteer registries,
148 patients' spouses or partners and patients attending the clinic for reasons other than
149 glaucoma (for example, for preoperative assessment for cataract in the fellow eye).

150 If deemed eligible for the study, healthy subjects were recruited consecutively.

151 Both eyes were examined but only one eye per subject was used in the final analysis, chosen
152 randomly if both eyes were eligible. All patients gave their written informed consent to
153 participate in the study. Ethics Committee approval was obtained (International Ethics
154 Committee of Milan, Zone A, 22/07/2015, ref: Prot. n° 0019459) and the study was registered
155 as a clinical trial (ISRCTN13800424). This study adhered to the tenets of the Declaration of
156 Helsinki.

157 Each subject had an ophthalmological evaluation following a standard operating procedure
158 involving assessment of axial length (AL) measurement with the IOL Master (Zeiss) biometer,
159 SD-OCT of the Optic Nerve Head (ONH) and RNFL, perimetric demonstration (only for
160 subjects naïve to perimetry); one examination with HFA 24-2 grid SITA Standard to both eyes
161 and one examination with CMP New Grid (see below), ZEST strategy to both eyes; colour
162 fundus photo with CMP.

163 The reference standard to diagnose GON was clinical evaluation by an expert based on RNFL
164 SD-OCT and/or optic nerve head photography. The rationale for this choice was to avoid any
165 classification based on VF testing that could have affected the analysis of the relative
166 discriminative power of the index tests. The two index tests were VF examinations with the
167 HFA and the CMP. The order of CMP and HFA tests was randomized. The VF examination
168 performed with the HFA used a 24-2 grid and the SITA – Standard algorithm. Near correction
169 was used. Fixation was monitored with blind spot tests using the Heijl-Krakau method ⁸.

170 The VF examination performed with the CMP employed a testing grid termed ‘New Grid’
171 which differs from the HFA 24-2 grid (Supplementary Figure 1, available at
172 www.aaojournal.org). The New Grid contains all the 52 locations tested with a 24-2, only one
173 blind spot location (instead of 2 as in the 24-2) and 12 additional points in the macular region
174 of the VF. The testing strategy was an adaptation of the Zippy Estimation by Sequential
175 Testing (ZEST) ^{9,10}. Since the CMP is equipped with autofocusing, no near correction was
176 needed. Blind spot responses were monitored by projecting stimuli on the location of the
177 ONH, identified manually by the operator on the baseline infrared fundus image captured at
178 the beginning of the test. In all the analyses, only the 52 locations in common between the 24-
179 2 and the New Grid were used.

180 For both devices, VF examinations were considered reliable if the false positive frequency
181 (FP) was $\leq 18\%$ and the Blind Spot response frequency (BP) was $\leq 25\%$. If either the HFA or

182 the CMP VF was deemed unreliable, the eye was excluded from the analysis.

183

184 *Statistical analysis*

185 All analyses were based exclusively on the 52 locations in common between the 24-2 grid
186 (HFA) and the New Grid (CMP).

187 Differences between the two devices in terms of Mean Sensitivity (MS) and its decrease with
188 age in healthy subjects were analysed. Since the same eyes were tested with both devices, a
189 mixed model was used to account for repeated measurements.

190 Linear regression was used to estimate expected decrease in sensitivity with age in healthy
191 subjects (dB/years) at each VF location. Total deviation (TD) values for each VF in normal and
192 glaucoma subjects were calculated as the deviation from the mean trend in the age model for
193 each location. Mean Deviation (MD) was calculated as the mean of all 24-2 grid TD values in
194 each VF. Mixed models were used to compare MS and MD values between the two devices in
195 both the glaucoma and normal groups. MD values were only compared for the glaucoma
196 group since subjects in the normal group were used to calculate the TD values and are bound
197 to have a mean MD equal to zero with both devices.

198 Normative lower limits for each location were calculated for TD values using quantile
199 regression ^{11, 12} to account for changes in normal variability with age. Since the variability of
200 thresholds in healthy subjects is known to increase with age ^{12, 13}, we only allowed for
201 negative slopes in quantile regression, meaning that normative limits could not shrink with
202 age. Only the lower 5% and 1% limits for TD values were used in this analysis.

203 For a fair comparison, TD values and their normative limits were calculated in the same
204 fashion for HFA and CMP, using the dataset of healthy subjects acquired with each respective
205 device in this study.

206 For each VF, we calculated the total number of TD values below the 5% and 1% limits, which
207 we refer to as TD 5% and TD 1% respectively.

208 Discrimination ability of the two index tests was measured using MD, TD 5% and TD 1% as
209 classifiers. These classifiers were used to build Receiver Operating Characteristics (ROC)
210 curves. Instead of comparing the whole ROC curve, we analysed the Partial ROC curve (pROC)
211 down to a minimum specificity of 0.75 to avoid comparing the two devices at too low
212 specificity values that would fall far outside a clinically useful range. The 95% confidence
213 intervals for Partial Areas Under the Curves (pAUCs) and p-values for differences were
214 calculated via bootstrapping¹⁴.

215 The normative data, used to calculate MD and TD metrics and their normative limits, was
216 composed of the same set of healthy subjects used in the discrimination analysis to calculate
217 pROC curves and their pAUCs. Therefore, they are only used here to compare the relative
218 performance of the two devices and not to estimate or report their actual discriminative
219 power.

220 To compare test times, CMP average time per location was calculated for each test and the
221 result multiplied by the number of total points in a 24-2 grid (54 points). This made it
222 comparable with the testing time read from the printout of the HFA.

223

224 *Data collection for test - retest variability*

225 A separate group of glaucoma and healthy subjects was recruited to assess test – retest
226 variability with the two devices. The target number was 56 subjects with GON and 56 healthy
227 subjects. The sample size calculation for this part of the study was based on previously
228 reported data for test - retest in healthy subjects and glaucoma patients^{15, 16}. All subjects
229 underwent the same examinations reported for the previous section and the diagnosis of GON
230 was again confirmed by expert evaluation of the RNFL on SD – OCT images or photographs of

231 the optic nerve head. Subjects were sequentially recruited in the same way described for the
232 previous part of the study. No stratification by disease (VF) severity was planned in the
233 recruitment of glaucoma subjects. All subjects performed four VF tests: two with CMP with a
234 24-2 grid, ZEST strategy, and two with HFA with a 24-2 grid, SITA Standard strategy, in
235 randomized order. All examinations were done within a time span of seven days.

236

237 *Statistical analysis*

238 Test – retest variability for the overall VF was assessed for MS using Bland – Altman plots and
239 95% limits of agreement. Any change in test-retest variability was evaluated by percentage
240 reduction of the 95% interval of agreement of CMP over HFA. The 95% confidence intervals
241 for the percentage variation were estimated using a paired bootstrap procedure with 50000
242 resamples. Mean Absolute Deviation (MAD) was used to assess pointwise test - retest
243 variability. Differences in MAD, point-wise sensitivity and MS were tested using t-test
244 statistics from linear mixed models with random effects to account for correlations between
245 VF measurements from the same subject.

246 All analyses were done using R version 3.3.1 (R Foundation for Statistical Computing, Vienna,
247 Austria).

248

249

250 **Results**

251 *Normative database*

252 For this part of the study, 1249 people were screened for eligibility and invited to participate
253 between 14/09/2015 and 31/07/2017. Of these, 177 subjects did not satisfy the inclusion
254 criteria and 59 did not complete the examination protocol. Finally, 70 subjects were excluded
255 because they had at least one unreliable VF test (48 with HFA, 20 with CMP and 2 with both
256 devices).

257 Therefore, 444 healthy subjects and 499 glaucoma subjects (patients with GON) were
258 included in the final analysis. Although no stratification by disease severity was planned, a
259 wide spectrum of VF severity was obtained by the end of the recruitment. Glaucoma Staging
260 System 2 (GSS2)¹⁷ stage distribution for glaucoma participants is reported in Table 1 and
261 depicted in Figure 1.

262 Subjects' age distributions are reported in Table 1. Mean age (\pm standard deviation [SD]) was
263 48 ± 16 and 68 ± 11 years for the normal and glaucoma group respectively.

264 Average MS was lower with CMP compared to HFA in healthy subjects (Mean \pm SD, 27.6 ± 1.6
265 dB vs 29.4 ± 2.0 dB) and glaucoma subjects (20.5 ± 6.7 dB vs 21.9 ± 6.9 dB) and these
266 differences were both statistically significant ($p < 0.001$). Comparison of the MD values in
267 healthy subjects has not been performed since this group was used to calculate the normative
268 average and therefore they were bound to have zero means for both devices. The MD values
269 from the two devices showed good agreement (Figure 2). Indeed, the average MD (\pm SD) for
270 glaucoma subjects was -6.55 ± 6.60 dB (Median: -4.37 dB, IQR: 8.92 dB) with CMP and $-6.50 \pm$
271 6.63 dB (Median: -4.73 dB, IQR: 9.19 dB) with HFA and this difference was not statistically
272 significant ($p = 0.54$).

273 Average number of presentations (\pm SD) per location in CMP was 3.02 ± 0.55 for healthy
274 subjects and 3.70 ± 1.09 for glaucoma patients. Corrected test duration for CMP and test
275 duration for HFA were similar in both the healthy and glaucoma subjects (see Table 2).
276 Point-wise sensitivity was generally lower for CMP compared to HFA (Figure 3). The average
277 mean difference was 1.85 ± 0.06 dB (Mean \pm Standard Error, $p < 0.001$) in healthy subjects
278 and 1.46 ± 0.05 dB (Mean \pm Standard Error, $p < 0.001$) in patients with glaucoma. Similarly to
279 the MD, such a difference was reduced when total deviations were considered in glaucoma
280 subjects (Figure 4), with 7 locations exceeding 1 dB difference.
281 The MS in the healthy group decreased with age in a similar fashion for both devices, with a
282 small but statistically significant difference (-0.051 ± 0.005 dB/year for HFA and $-0.027 \pm$
283 0.005 dB/year for CMP; Mean \pm Standard Error; $p < 0.001$ for slope difference).
284 The rate of false positives was 1.6 ± 4.0 % for CMP and 1.6 ± 2.3 % for HFA (Mean \pm SD).

285

286 *Discrimination analysis*

287 Relative discriminative power (relative diagnostic precision) was marginally greater for CMP
288 when compared to HFA using the MD metric (pAUC difference \pm Standard Error, $0.019 \pm$
289 0.009 , $p = 0.035$, see Figure 5). There was no statistically significant difference in pAUC
290 between CMP and HFA when using TD 5% ($p = 0.18$) or TD 1% ($p = 0.22$) as the classifier.
291 Sensitivity values at selected specificities are reported in Table 3.

292

293 *Test – retest variability*

294 By the end of the study, 99 subjects were screened; one subject did not complete all the
295 examinations and was excluded. In total 54 healthy subjects and 44 glaucoma patients, were
296 recruited for the test – retest study. Bland – Altman plots are reported in Figure 6. The mean
297 difference in MS between the first and the second test with the CMP was statistically different

298 from zero in glaucoma subjects (Mean \pm Standard Error, 0.44 ± 0.21 dB, $p = 0.041$). Bootstrap
299 distributions of the percentage improvement for the glaucoma group are reported in
300 Supplementary Figure 2 (available at www.aaojournal.org).

301 The 95% limits of agreement for MS are depicted in Figure 6. They were 49% (95% CIs: 17%
302 to 67%) narrower for CMP (Limits of agreement: -1.31, 1.63 dB) compared to HFA (Limits of
303 agreement: -2.84, 2.91 dB) in the healthy subjects. The 95% limits of agreement were 13%
304 narrower for CMP (Limits of agreement: -2.26, 3.14 dB) compared to HFA (Limits of
305 agreement: -3.11, 3.11 dB) in the glaucoma patients but the confidence intervals for these
306 estimates were very large (95% CI: - 28% to 42%). In glaucoma subjects, the mean test -
307 retest difference (\pm SD) was 0.44 ± 1.38 dB for CMP and 0 ± 1.59 dB for HFA. Bland - Altman
308 plots for all sensitivities are reported in Figure 7. The 95% limits of agreement were generally
309 narrower for CMP for sensitivities above or equal to 15 dB (Mean Difference: 1.80 dB,
310 between 15 and 30 dB) and larger below 15 dB (Mean Difference: 5.46 dB).

311 Pointwise test - retest variability, calculated using the MAD was not significantly different
312 between CMP and HFA for glaucoma patients (Mean \pm SD, CMP: 1.03 ± 1.01 dB, HFA: $1.07 \pm$
313 1.16 dB; Mean Difference \pm SE, 0.03 ± 0.2 dB, $p = 0.88$) and for healthy subjects (Mean \pm SD,
314 CMP: 0.59 ± 0.48 dB, HFA: 0.90 ± 1.15 dB; 0.08 ± 0.16 dB, $p = 0.62$).

315

316 **Discussion**

317 This study was designed to compare two index tests, CMP and HFA, in terms of test - retest
318 variability and relative discriminative power. We recruited a large cohort of 943 subjects (499
319 patients with glaucoma and 444 healthy subjects) for the discrimination analysis and 98
320 subjects (44 glaucomatous and 54 healthy) to compare test-retest variability. The reference
321 standard used for the diagnosis of GON was independent of VF assessment, based on
322 specialist assessment of ONH colour photography and/or peripapillary RNFL thickness
323 measured with SD-OCT.

324 The primary objective was to show a reduction of test - retest variability in the MS of at least
325 20%. Such a reduction was achieved in healthy subjects (49%), but not in glaucoma subjects,
326 where the reduction was of 13%. Several factors might have contributed to this result, such as
327 a more pronounced perimetric learning effect with CMP¹⁸⁻²¹. The mean difference in MS in
328 CMP between the first and the second test was small but statistically significant and this may
329 be indicative of a learning effect in the glaucoma test - retest cohort. This effect was not seen
330 in the HFA data. Indeed, despite all glaucoma subjects in our sample having had previous
331 experience with SAP, the new setup of a fundus perimeter might have created an unfamiliar
332 testing condition for test takers. In fact, most of them were recruited from glaucoma clinics
333 and were experienced with HFA. The different threshold acquisition strategies employed by
334 the two devices may also explain this difference. SITA strategies incorporate spatial
335 information between neighbouring test locations. Such an approach allows for faster
336 threshold estimation, but it has been shown to bias the estimates introducing correlations
337 between neighbouring points^{22,23}. On the other hand, the implementation of the ZEST
338 strategy used in CMP tests each point independently. Moreover, test - retest variability is
339 known to increase dramatically at lower sensitivities²⁴⁻²⁷ and this effect may simply consume
340 any improvements from adjusting for fixation stability afforded by the tracking in fundus

341 perimetry. We speculate this is the reason we see much bigger improvement in test-retest
342 variability in the healthy subjects compared to the patients in this study. This is supported by
343 the results shown in the Bland-Altman plots for pointwise sensitivities, where it can be
344 observed that the CMP offers no advantage in test-retest variability compared to HFA at
345 values below 15 dB. Indeed, the 95% limits of agreement between 11 and 14 dB were larger
346 for CMP than for HFA. The difference here might be explained by the spatial smoothing and
347 the use of growth pattern to seed the priors^{9,22} in the SITA strategy, which might play a large
348 role in reducing the test retest variability in this sensitivity range. However, the clinical utility
349 of thresholds below 15 dB has been questioned. Indeed, recent evidence suggests that
350 increasing perimetric contrast all the way to 0 dB may not be clinically useful and sensitivities
351 obtained at severely damaged visual field locations (<15-19 dB) are unreliable and highly
352 variable. It could be argued that improvements in tests-retest variability in the upper range of
353 sensitivity values could be more clinically relevant for progression detection²⁴⁻²⁹. However,
354 this is speculation because only analysis of long-term follow-up of glaucoma subjects with the
355 CMP will allow the assessment of the real effect of such reduction in variability on earlier
356 diagnosis of progression.

357 Additionally, Wyatt et al identified gaze instability as a possible source of variability at the
358 edges of scotomata³⁰, and tracking might help reduce this effect. However, their analysis was
359 performed with a 10-2 grid, which has a much finer spacing between locations (2 degrees).
360 Hence, further investigation is needed to assess the effect of gaze instability in the estimation
361 of edges on a typical testing grid, such as 24-2 or 30-2.

362 One limitation of our analysis is that the sample size of the glaucoma test - retest group was
363 probably too small to reliably assess any differences, as shown by the large confidence
364 intervals calculated via bootstrapping (Supplementary Figure 2, available at
365 www.aaojournal.org). Post hoc power calculations based on bootstrap resampling estimated

366 that 97 glaucoma subjects would have been needed to detect a 20% improvement at a
367 significance level of 0.05 with 80% power. This is considerably above the initial estimates
368 obtained from literature data ^{15, 16} used for designing of the study. Therefore, an additional
369 investigation with longer test series on a larger sample might be needed to fully assess the
370 effect of fundus tracking on test – retest variability.

371 Relative discriminative power for the two index tests (devices) was similar. When compared,
372 pROC curves calculated using the number of abnormal points per field in the TD maps largely
373 overlapped, with no evidence for any superiority of either index test (Figure 5). Statistically
374 significant differences in pROC curves were observed when MD was used as a classifier but
375 such differences are too small to be likely relevant in clinical situations. These results are
376 compatible with the fact that, although the actual sensitivity estimates were lower for CMP
377 compared to HFA, relative indices, such as the MD and TD values, showed only small
378 differences in glaucoma subjects between the two devices, yielding similar diagnostic ability.

379 Our results are based on a large sample of individuals from different centres. The different age
380 clusters, except for people older than 80 years of age, were well represented (Table 1). This
381 was sufficient to reliably conduct an analysis on relative discriminative power. It is important
382 to note that, for both devices, all indices used in the discrimination analysis (MD, TD 5% and
383 TD 1%) and the normative limits for TD were recalculated in the same fashion from the raw
384 sensitivities and are therefore comparable. However, since the normative limits have been
385 derived from the same group of healthy subjects used in the discrimination analysis, the
386 pAUCs are biased and can only be used to compare the relative discriminative ability of the
387 two devices; they cannot be generalised to estimate the effective discriminative power of
388 either the CMP or the HFA in clinical practice.

389 Examination times for the two devices were similar. Both devices took, on average, 5 to 6
390 minutes to complete. Testing times had to be corrected prior to comparison due to the greater

391 number of tested locations with the New Grid used with CMP (65 locations) compared to the
392 HFA 24-2 grid (54 locations). After corrections, no statistically significant differences could be
393 detected between the two devices in healthy subjects. A statistical difference was observed in
394 glaucoma subjects but it is clinically irrelevant (approximately an 11 second difference on
395 average). Despite similarities in overall examination times, fewer presentations were needed
396 to estimate thresholds in CMP when compared to HFA at the 52 matching locations. The
397 number of presentations in healthy subjects was 157 ± 28 , which is lower than that reported
398 for SITA-Standard in the literature (276 for 52 locations)¹³. Unfortunately, interpretation of
399 the examination times of the two devices is difficult for a variety of reasons. For example, CMP
400 uses catch trials whereas HFA SITA algorithms use response times to estimate false positive
401 error rates³¹. Moreover, the CMP does not project stimuli when the quality in the tracking
402 signal is low, and this may increase overall examination time.

403 One limitation of our study is that the glaucoma subjects were not stratified according to
404 disease severity, since VF data were not used in the diagnosis of GON. This could have
405 resulted in an uneven representation of glaucoma stages. However, the range of visual field
406 damage was sufficiently large to allow for a reliable evaluation across the whole spectrum of
407 glaucoma damage (see Table 1 and Figure 1).

408 Our recruitment of healthy subjects was not population based and this is another potential
409 limitation of our study. The main design bias potentially recruiting 'super-normals' in studies
410 of diagnostic precision is to recruit the healthy control group using restriction criteria related
411 to the outcome of interest³², for example requiring the healthy controls to have normal visual
412 fields. We explicitly avoided this bias. Nevertheless, volunteers to clinical studies may be
413 healthier than an unselected population. This is very hard to avoid, because participants need
414 to volunteer. However, when we analysed the MD values from the HFA printouts of the 444
415 healthy subjects, whose calculation is based on the independent internal normative database

416 built in the device, we found that our sample did not show important deviations from the
417 normative values. Indeed, the average MD was -1.12 ± 1.64 dB (Median: -0.91 dB, IQR: 1.97
418 dB).

419 Finally, the design of this study only allowed for a relative comparison of discriminative
420 power. Evaluation of the actual diagnostic accuracy would need a further validation on an
421 independent dataset, to assess how much these findings can be extracted on the general
422 population. Furthermore, such an evaluation should be conducted on a set of subjects before
423 the reference test (the clinical diagnosis of GON) is performed, as case-control scenarios are
424 known to produce biased estimates in discrimination analyses. One option might be to test
425 glaucoma suspects with the CMP before they are diagnosed as healthy or as having glaucoma.
426

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506

507 **Figure Legends**

508 **Figure 1.** GSS2¹⁷ plot showing the distribution of the 499 subjects with glaucomatous optic
509 neuropathy in the different stages of the classification. The light grey lines indicate the
510 boundaries for the different stages. Subjects are classified based on their MD and PSD values

511 directly taken from the HFA printout. The distribution is approximately uniform across the
512 different stages.

513

514 **Figure 2.** The two panels show the agreement of MD (on the left) and MS (on the right) values
515 between CMP (vertical axis) and HFA (horizontal axis). The black solid line indicates the ideal
516 perfect agreement. The red dots represent the healthy subjects while the green dots indicate
517 glaucoma subjects. Differently from MS, MD values did not show important differences
518 between the two devices.

519

520 **Figure 3.** Average sensitivity (dB) for each of the 52 locations considered in this analysis for
521 CMP (A) and HFA (B). The bottom panels report the average pairwise difference per location
522 in the healthy subjects (C) and for glaucoma patients (D).

523

524 **Figure 4.** Average total deviation value (dB) for each of the 52 locations considered in this
525 analysis for CMP (A) and HFA (B). Panel C reports the average pairwise difference (CMP –
526 HFA) in Total Deviation per location in the glaucoma subjects (in bold all differences
527 exceeding 1 dB).

528

529 **Figure 5.** Partial ROC curves built using the MD (in the leftmost panel) as a classifier. The
530 middle and rightmost panels depict partial ROC curves built using the number of abnormal
531 locations at two different cut-offs, 5% and 1%, on the probability maps for TD values. There
532 was no significant difference in either the TD 5% or the TD 1%. MD = Mean Deviation; TD =
533 Total Deviation.

534

535 **Figure 6.** Bland – Altman plots for MS. Red dots represent MS measurements from the HFA,
536 blue dots from the CMP. The shaded grey area indicates the 95 % limits of agreement on the
537 test-retest difference. The black solid line indicates the mean difference between test-retest
538 MS measurements. A small offset in the mean difference can be detected in the glaucoma
539 group with the CMP (bottom – left panel).

540

541 **Figure 7.** Bland – Altman plots for all sensitivities. Red dots represent MS measurements from
542 the HFA, blue dots from the CMP. The shaded grey area indicates the 95 % limits of agreement
543 on the test-retest difference. 95% Limits of agreement were narrower for sensitivities above
544 or equal to 15 dB, larger between 11 dB and 14 dB and equivalent below 10 dB. The larger
545 range in the differences was at 14 dB (-27 dB, 27 dB) for CMP and at 12 dB (-24 dB, 25 dB) for
546 HFA.